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瑞棋 陳

道昌徐

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# 電腦化肌電圖之定量分析簡介

#### 陳瑞棋 徐渞昌

### 一、前

Licht S. 在其Electrodiagnosis and Electromyography(1)一書中即指出,早在一 八四二年, Dubis-Reymond 即發現人類的肌 肉可產生電流。一八五一年,他作了第一個人 類的肌雷圖檢查。其後肌電圖的知識及裝備逐 步改進。一九〇九年; Lapicque 定下了"Rheobase "及 "Chronaxia " 的名稱。一九一六 年Adrian 報告了第一個人類的《力量一間期 曲線"。一九二二年,陰極射線管被用於肌電 圖的示波器。一九二九年 Adrian 製成了同軸 **針極,並裝設擴音器以輔助檢查。一九四四年** ,單極針極問世。一九五三年,由Lambert 首創神經傳導速度的檢查方法。雖然有很多人 一直致力於肌電圖的定量分析,但是大部分僅 限於直接觀察示波器中的電波,或用紙記錄下 一連串的肌電波而後以人工量其波幅、問期、 相數等(2)。不但費時費力,而且主觀因素的影 響很大,所報告的數值變動幅度也甚鉅(見表 一)(1)~(8)。彼時因囿於對解剖及電機知識瞭 解有限,肌電診斷學無法得以有突破性的進展 ,而始終停留在半定量的階段。甚至於需藉戰 争造成的傷患檢查才得以流行一陣子(1)。這種 情形直到二次世界大戰之後才改觀。

#### 二、電腦化肌電圖的演進及簡介

自從Liddell 及 sherrington 於一九二 五年定下運動單位(Motor Unit)的名稱以 後,肌電圖的檢查及解釋即以運動單位的發現 爲依據,肌電圖的定量分析研究也多以運動單 位爲中心。自一九五〇年代以來,卽有很多學 者提倡各種不同的自動分析方法,目的便是要 使肌電圖的判讀數據更爲客觀可靠而且可以再 現( Reproducible )(4)。一九五一年Richardson 提出了頻率的自動分析(7); Lenman

使用表面電極記錄肌肉的輸出功及負重的比率 (8);一九六七年 Fitch 藉電子分析 來量 度干擾 狀況的波數和波幅變化,這些都是最早期的肌 電圖自動化分析的報告。 Eberstein 及 Goodgold 對肌電圖的定量分析有極有系統的描述 (9)。他歸納近代自動化定量肌電圖檢查多是朝 著(1)衡量個別動作單位之波幅、間期、波型及 點發型態。②衡量多數動作單位一齊點發時之 

(1)個別動作單位之衡量:每條肌肉包含了 100 至 1000 個動作單位(3)(0); 故要記錄單獨 的動作單位電波實屬不易。在以往唯有令病人 盡量放鬆肌肉,只作最輕微的收縮,而用肉眼 直接由示波器判讀,然而病人往往無法完全合 作,而且傳統的流動記錄方式經常會誤將早期 的神經病變肌電波誤認為是肌肉病變,也不可 能看出神經再生時所早現的遠端小波( Late Component ) 及顧移現象(Jittering)。於 是有各種新的方法及裝置來改善(9)。最重要的 關鍵則在於選擇適當的動作單位電波,並予以 固定於螢幕而重複記錄,以消除其他散在的雜 波,前者可藉激發裝置(Trigger Mode)達 到目的(11),後者則要加上平均裝置(Average Mode ),而且爲了認清整個波型,常要附加延 遲線(Delay line)以使電波顯示在螢幕之 某一固定位置(12)(13)。取得單獨的動作單位電波 後,即可將訊息輸入電腦予以記錄及計算。在 文獻報告中用於肌電圖的電腦種類很多,如A-NOPS (14) , BIOMAC 1010 (15) , DIGITAL Equipment Corporation PDP8 (11) , PDP12 (16) , P-DP 11 / 40 (17) , PDP 11 / 55 (18) , PDP 12 -A - 8K memory (11) • Cyber 73 (19) • HP 2100 (20), BIOMAC 500 (21)…等等,由於所用的電腦 及程式不同, 所記錄的動作單位的數據及其定 ·義也就不一樣,不外是計算其波幅(Amplitude )、間期(Duration)、相數(Phases ) •

)、點放方式( Firing Pattern )(9)。最近 瑞典的 stalberg 氏設計了一套可連接於 Apple 【電腦的程式,比前述數種方法更爲新顯 · 完備而且實用, 當運動單位訊息經過肌電圖 機的激發,平均處理後輸入電腦,即可由程式... 自動算出下列各項數據:①波幅:係衡量尖端 至尖端 (Peak To Peak )的幅度。②間期: 由動作單位電波離開基線 15 uV 以外開始,至 回到基線 15 uV 以內之期間。③表面積:係動 作單位電波所包含的表面積大小,單位是 MV ×MS, ④相數:爲動作單位電波通過基線的次 數。⑤轉折數(Turns):爲動作單位電波轉 撥版向而其幅度大於 50 uV 之次數。⑥尖端間 期(Peak Duration):係第一個至最後一個 轉折之間的間期。①至③項與動作單位的大小 有關, ④至⑥項則與動作單位電波的複雜性有 關。每條肌肉記錄 20 至 30 個動作單位後即可 算出各項數據的平均值及標準差。所有數據皆 可貯存於另一電腦軟體記憶卡中,非常適合臨 床之檢查及統計、比較、分析等研究。例如神 經病變患者,其動作單位的各項數據皆有偏高 的趨勢,而且與正常人之數據相差具有統計學 上的意義,我們由電腦資料看到的,不但客觀 、可靠,可以逐項定量比較,更可以進而推知 動作單位的病理變化。

(2)干擾狀態(Inter-ference Pattern)之衡量:干擾狀態係指多數動作單位同時點放時之結合情形。Willison 首先使用一定重量加於肌肉,而用電腦紀錄其轉折數及綜合波幅等情形(2) Fuglsang — Frederiksen及Masson 亦利用電腦計算肌肉作不同程度的收縮時之轉折、波幅及間期之關係(2);而 Hirose,Uono及 Sobue 用相同方法比較了神經病變與肌肉病變患者不同之干擾狀況(2);其後干擾狀況的研究雖然續有論文發表,但並無重大突破卻一份。直到一九八二年,Cenkorich,Hsu及Gersten發表了新的論點(3),他們經由電腦即便可能與係,此關係並不因肌肉之收縮程度不同而受影響。而在此同時,stålberg及

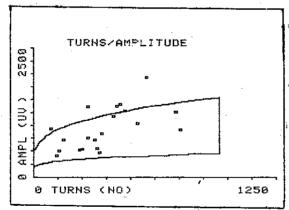
另外神經傳導的檢查也已邁入電腦化,當電刺激產生之肌電波出現於螢幕,電腦即可自動定出其潛期(Latency)及波幅,再刺激近端得到另一個電波,量好兩點間的距離輸入電腦,即可在螢幕上看到神經傳導速度;若所得的數值不在正常範圍時會有聲音警告,此可提醒檢查者重估其檢查步驟是否正確無誤。當神經傳導檢查完畢後,一份完整的報告便自動打出。

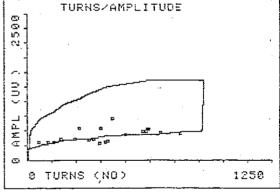
### 三、結語

表一 Normal Values of Motor Unit Potential Parameters:

	Amplitude (mv)	Duration (msec)	Polyphasic	Wave Form (phases)
Cohen	500-3,000	2-10	< 5 %	2-3
Marinacci	50-1,500	5-15	3 %	2-3
Smorto	100-1,000	3-15	2-12 %	3
Litch	100-2,000	2-10	1-12 %	2-3
Goodgold	300-5,000	3-16	< 10 %	2-3
Chu*	$675 \pm 11$	$15.2 \pm 0.2$	13.03 %	3.34

\*: Computer reading from Biceps (long head), monopolar needle, average datas of 660 motor units. Using Dr. Stalberg's computer program.





Neurogenic Turn-Amplitude Test.

Myopathic Turns-Amplitude Test.

#### Abstract

The purpose of this paper is to introduce recent developments of automatic quantitative analysis of electromyography using computer reading. Retrograde tracing of the trend of electro-myographic evolution both in concepts and instrumentations were documented. Advanced computerized analysis of single motor unit potential, interference pattern and nerve conduction studies were also illustrated briefly.

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